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# Low-Field Nuclear Magnetic Resonance Fingerprinting aided by Artificial Intelligence

## PROOF OF CONCEPT

PON Seminars - April 21, 2023

Workshop on Food Quality Analysis with Time Domain NMR and AI-Driven Mathematical Models

# Overview

- Why Nuclear Magnetic Resonance Relaxometry?
- What is Magnetic Resonance Fingerprint (MRF) technique?
- Why Artificial Intelligence?
- Low-field MRF relaxometry Framework
  - The approach
  - Proof of concept
- Conclusions



# Why NMR Relaxometry?



Composition and internal structure of dairy products

e.g. Quality:

pH

Viscosity

Water holding

Oxidation

Matrix...



*can be characterized by*

NMR relaxometry parameters ...

$T_1$

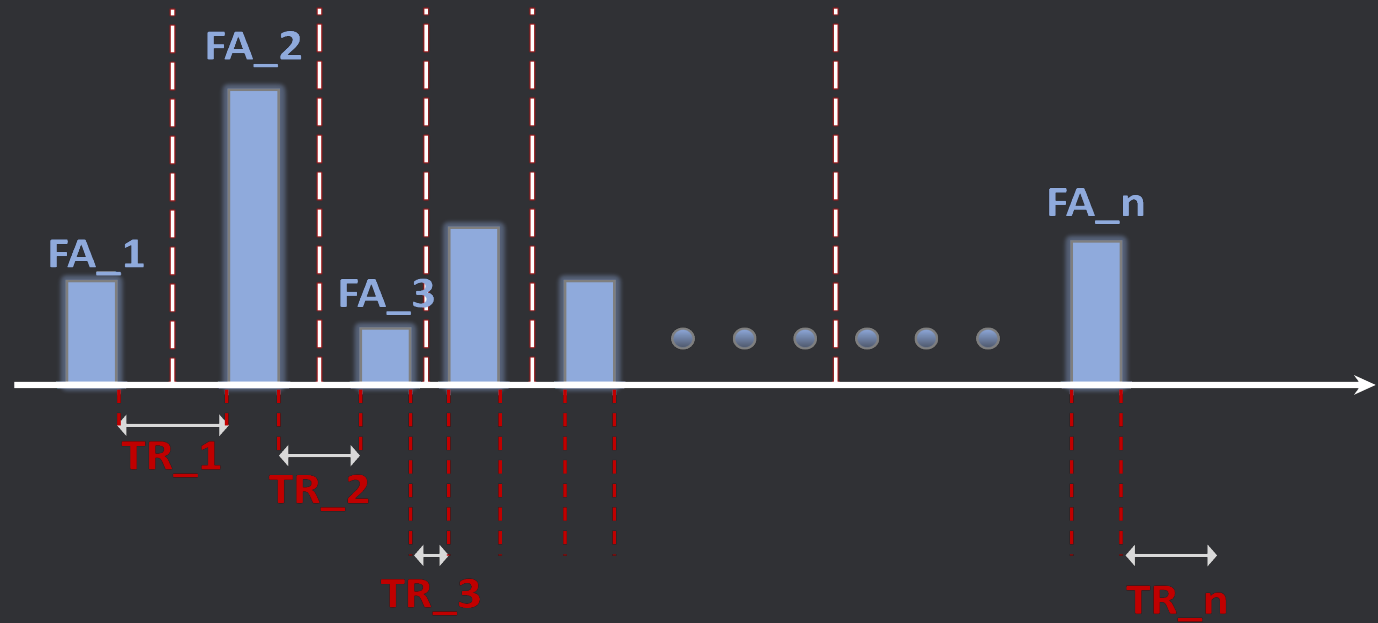
$T_2$

D

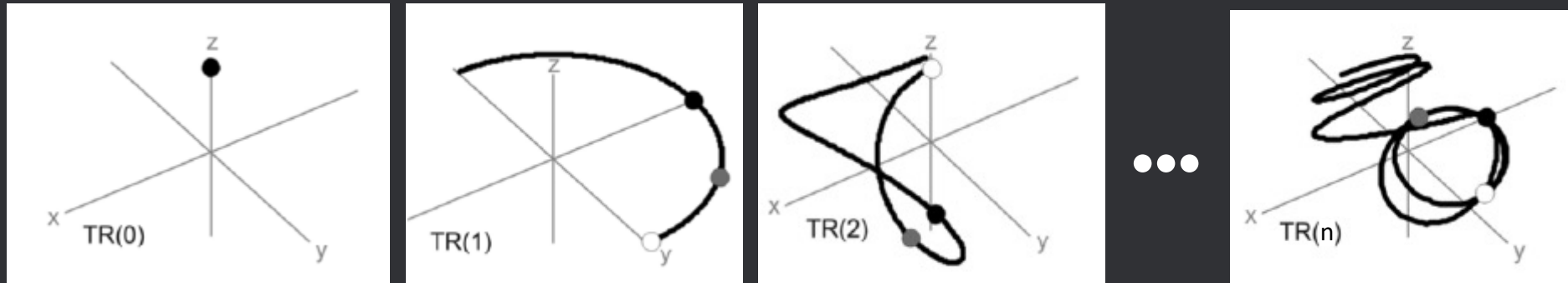
Solid/Liquid Ratio ...

# What is Magnetic Resonance Fingerprinting (MRF) technique?

RF Pulse Sequence

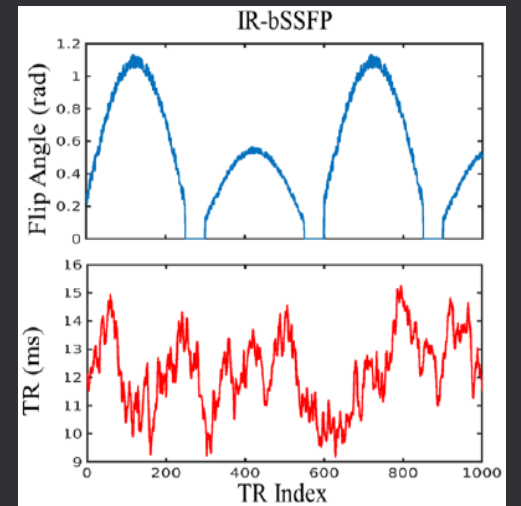
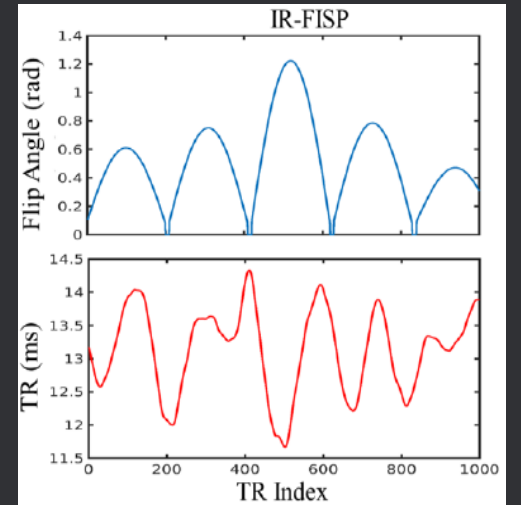
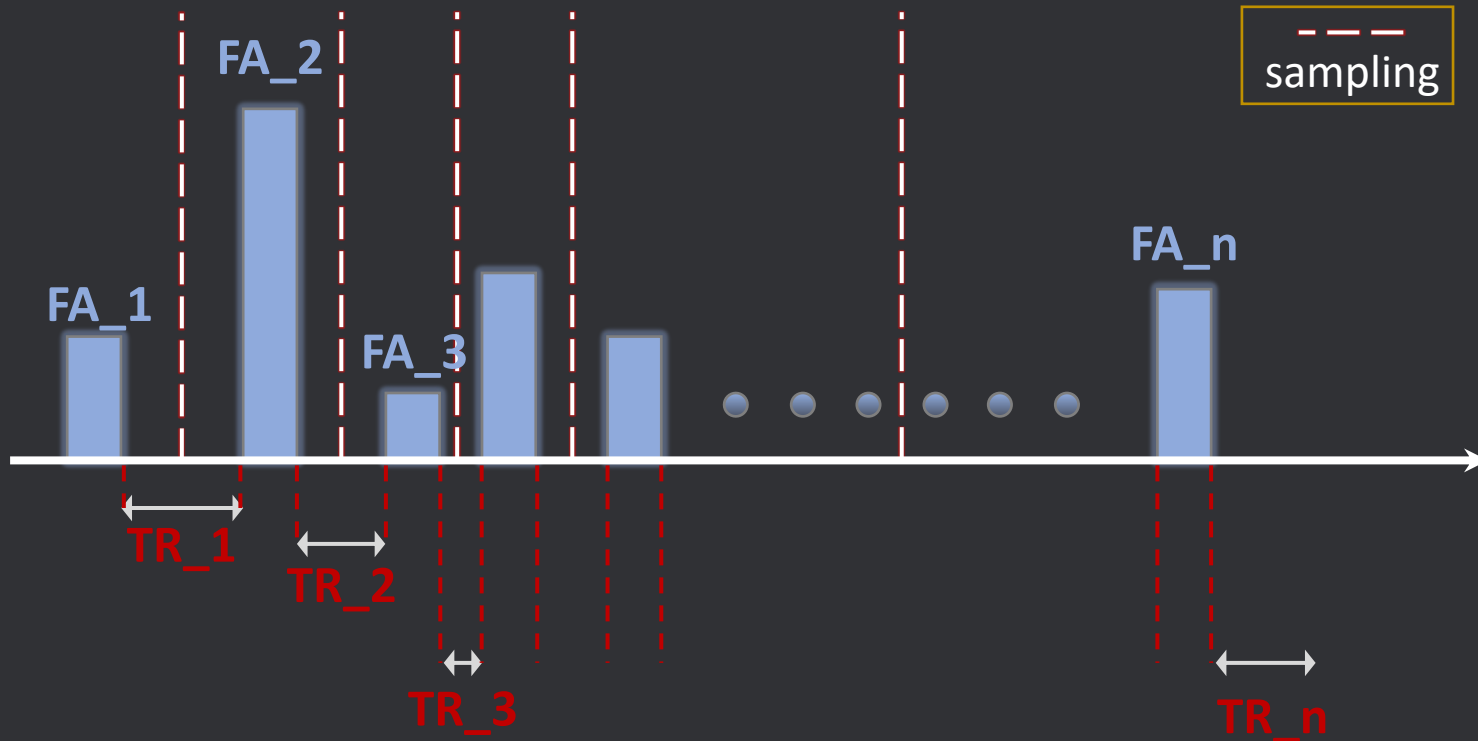


Bulk Magnetization evolution



# Magnetic Resonance Fingerprinting - Sequence design

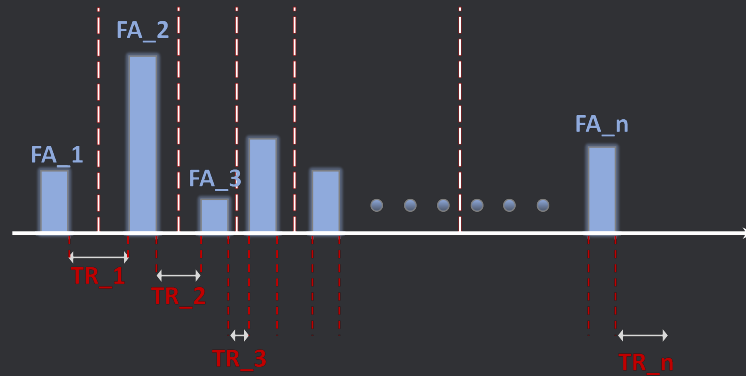
RF pulses: flip angle (FA) and repetition time (TR) vary according to a pattern designed to make the magnetization evolution sensitive to several MR parameters simultaneously.



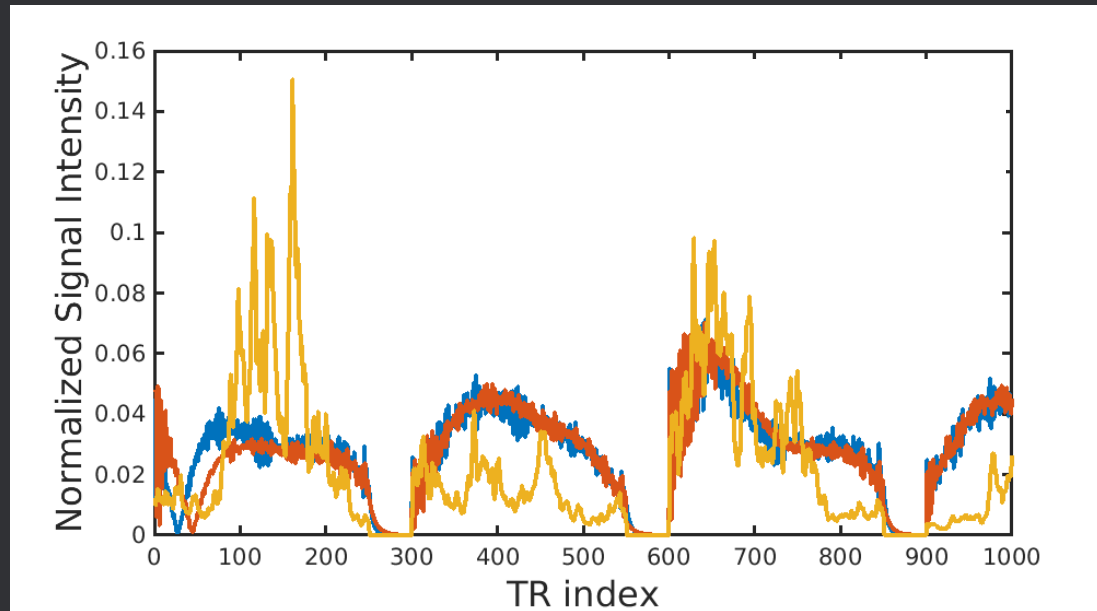
Examples of Flip Angle (FA) and Repetition Time (TR) of MR Fingerprint sequences

# Magnetic Resonance Fingerprinting approach to MR parameter mapping

RF Pulse Sequence



NMR Signal



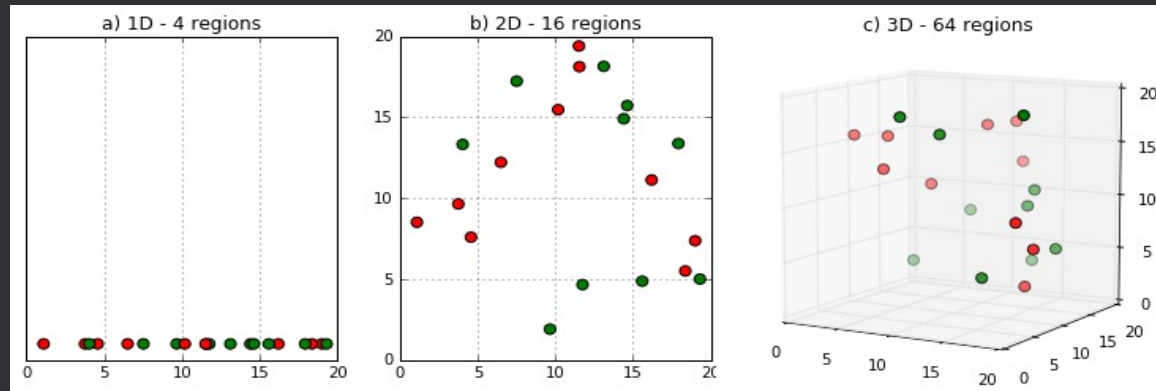
Examples of Fingerprint Signals varying  $T_1, T_2$  parameters

## Parameters estimation

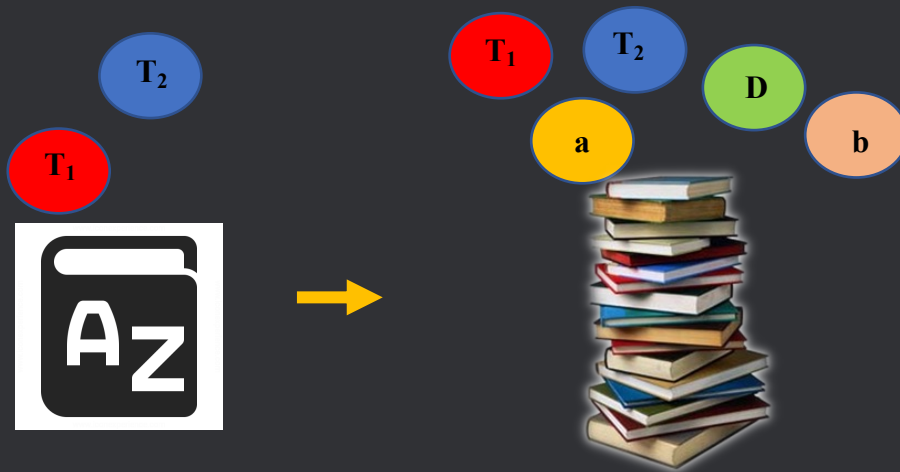


Simulating a dictionary with possible evolutions given a set of NMR parameters

# Circumventing The Curse of Dimensionality in Magnetic Resonance Fingerprinting with Deep Learning

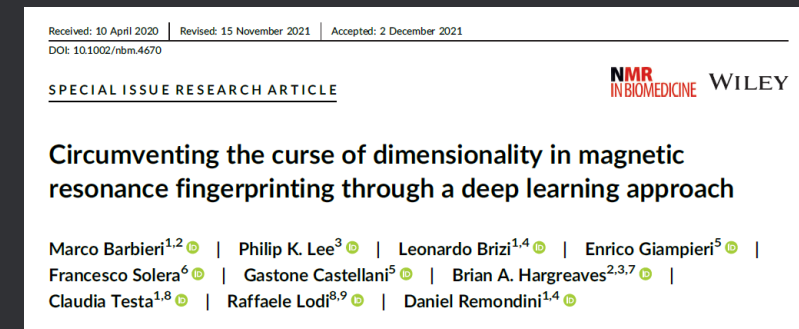


## The curse of dimensionality



Memory inefficiency and computational burden limit the scalability of MRF

The more parameters are added the bigger the dictionary becomes if no drops in accuracy is wanted.

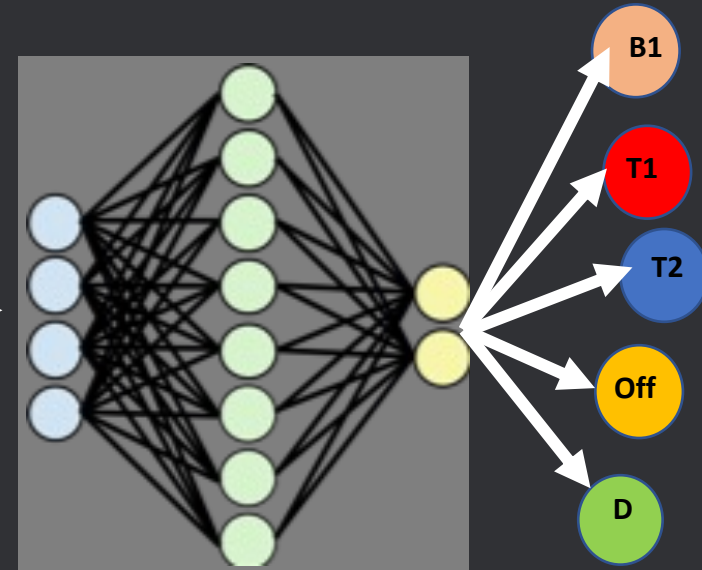


# Circumventing The Curse of Dimensionality in Magnetic Resonance Fingerprinting with Deep Learning

## Circumventing the curse of dimensionality



Experimental Signal →

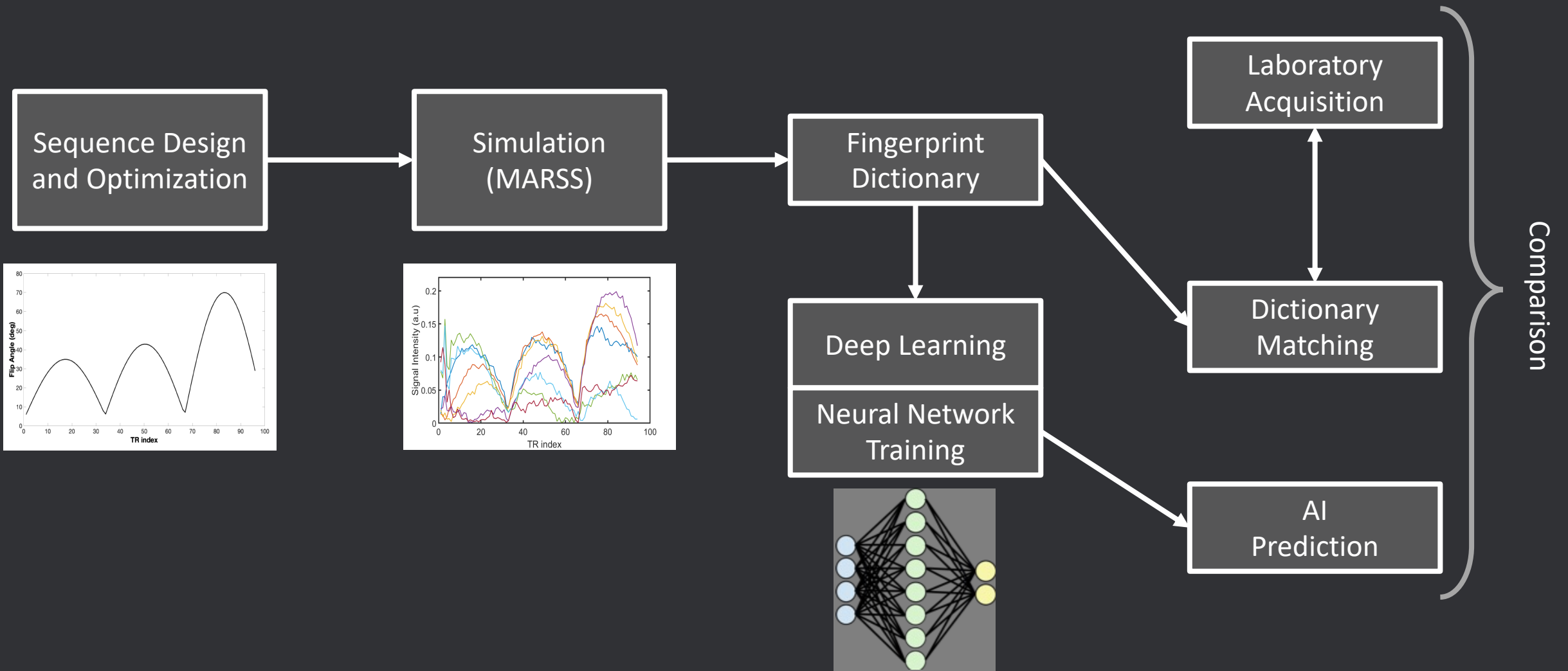


We can train a Neural Network to retrieve MR parameters given the MRF signal as input

→ **Adding parameters to be retrieved does not affect processing time.**



# Low-Field NMR Fingerprinting aided by Artificial Intelligence



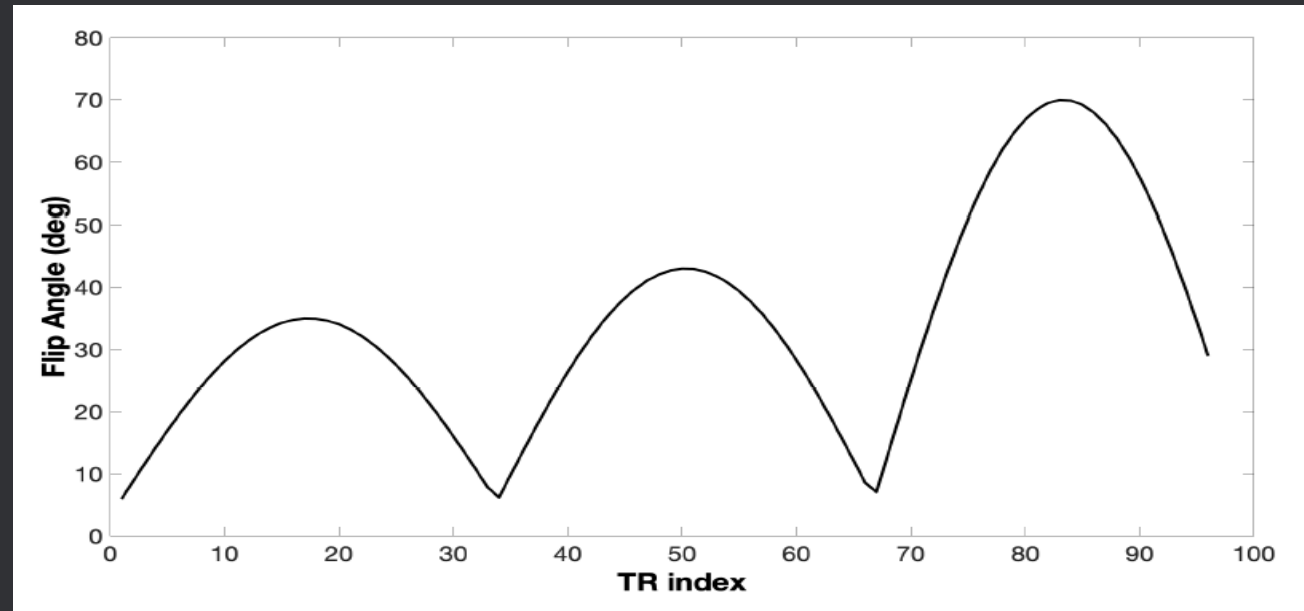
# Low-Field NMR Fingerprinting aided by Artificial Intelligence

## Sequence Design

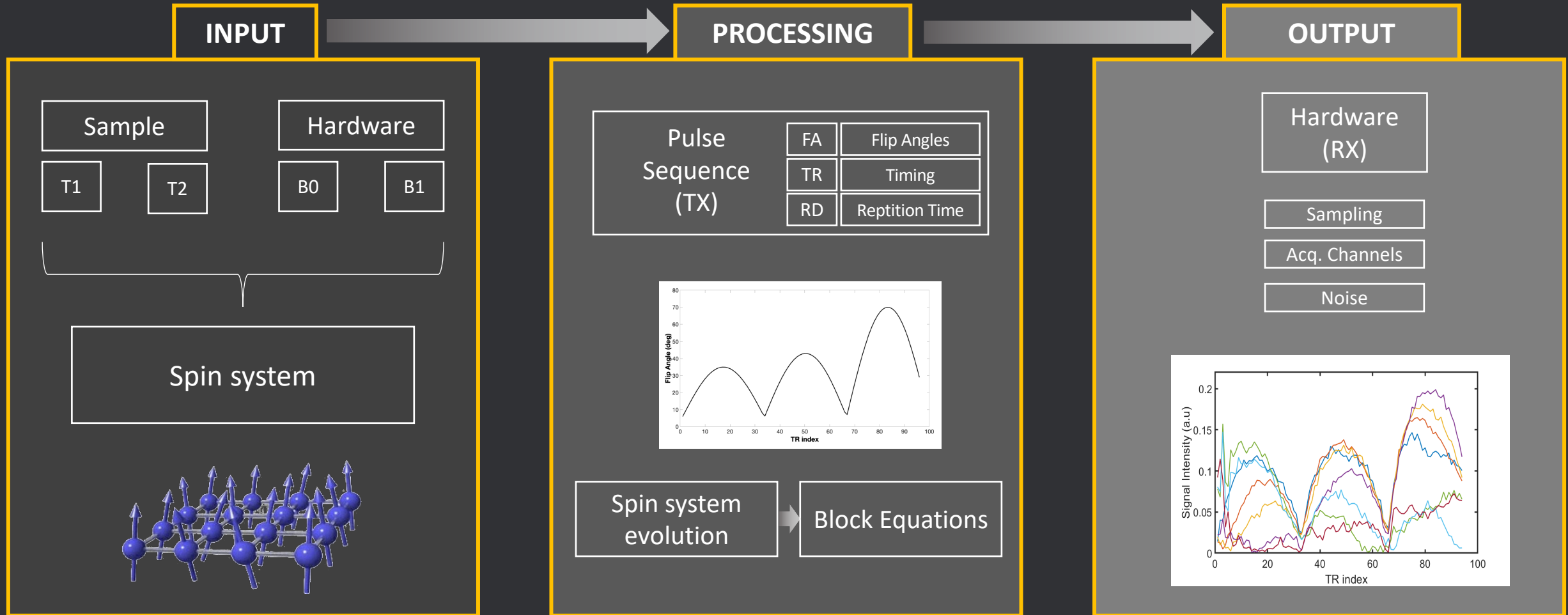
Time between pulses (TR) → fixed at 1 ms

Acquisition Time → fixed at the half of TR

Flip Angle Pattern (FISP-like)



# MARSS<sup>1,2</sup> (MAGnetic Resonance Simulation Software)



1) "MR Fingerprinting for partial volume fractions quantification: A simulation study", 103° Congresso Nazionale SIF, Trento, 11-15 sept 2017.

2) "Quantification of partial voxel volume fraction in a two-component system with a short T2 component: a UTE-MR Fingerprinting simulation study", 8° Congress AIRMM - Italian Chapter ISMRM, Gaeta, 8-9 june 2017.

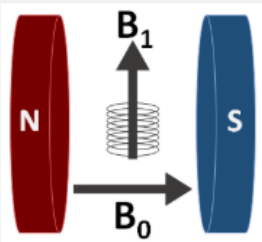
## NMR APPARATUS - SETUP panel

## External Magnetic fields characterization

Load B0-B1 map  
from datafile

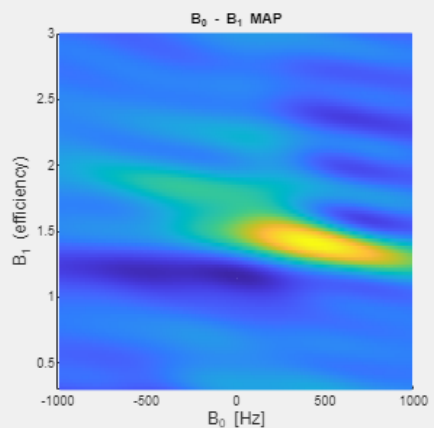
OR

## B0-B1 2DFFT of ANGLE-FID

LOAD >>> Compute  
B0-B1 MAP

	Min.	Max.
B0 range	-1000	1000
B1 eff. range	0.3	3
Inversion sizes	B0 400	B1 100

Export B0 - B1 MAP



Spin system components 4e+04

## Sample characterization

Relaxation Time T1 (s) 0.01

Relaxation Time T2 (s) 0.009

Signal-to-Noise Ratio 1000

SAMPLE



SETUP Apparatus  
Place the Sample into the Field

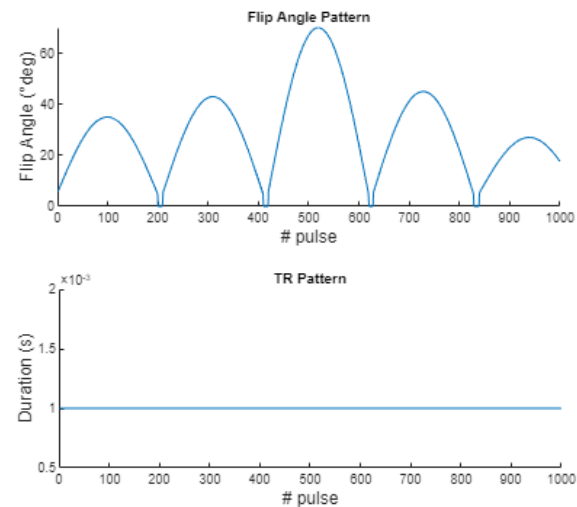
## EXPERIMENT SETUP PANEL - RF pulse sequence

MRF - IRBSSFP FID ANGLE CPMG IR-FID Inversion Recovery

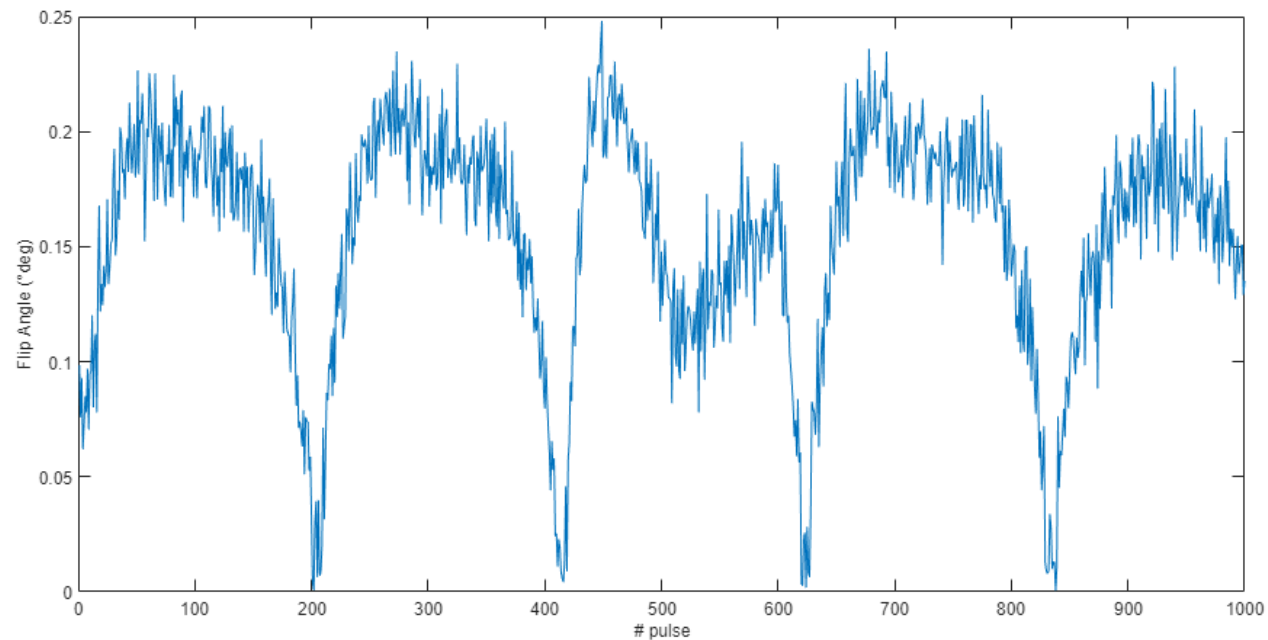
## Experiment parameters

Flip Angles Pattern	1	LOAD FAs
TRs Pattern	1000	LOAD TRs
Number of Sampling Points	4000	
Inversion time (s)	0.001	
Repetition Time (s)	10	
Number of scans	16	

RUN MRfingerprinting



## OUTPUT - NMR SIGNAL



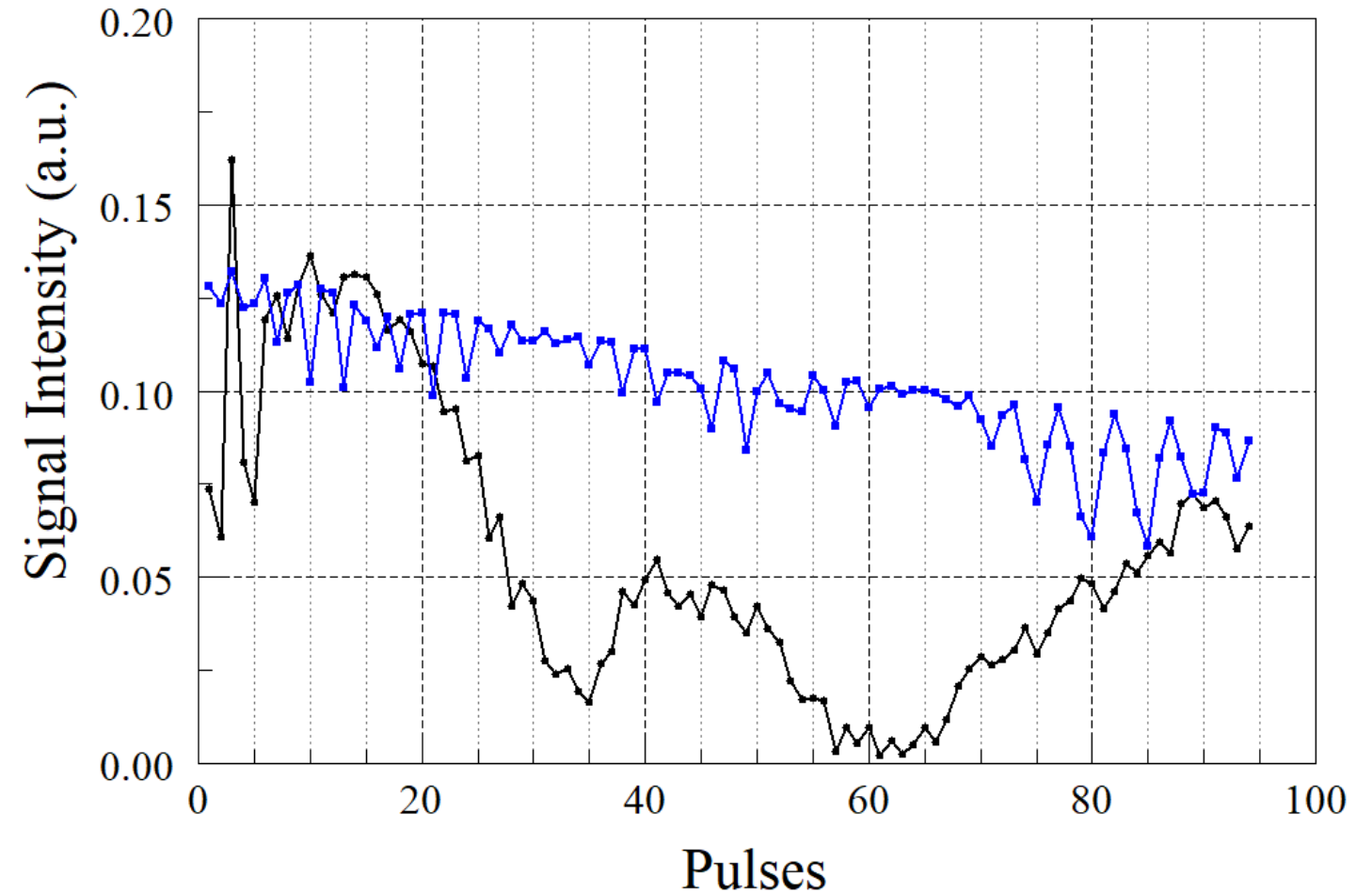
# Low-Field NMR Fingerprinting aided by Artificial Intelligence



Early challenging results...

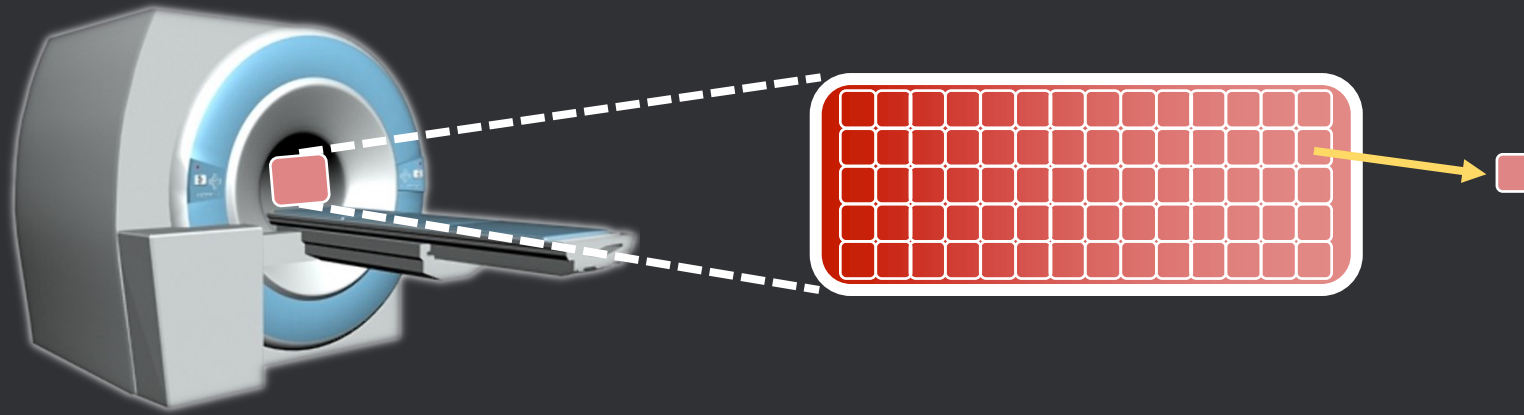
Acquired Signal  
Known T1,T2

Simulated Signal  
with known T1,T2  
(using single  $B_0$ - $B_1$ )



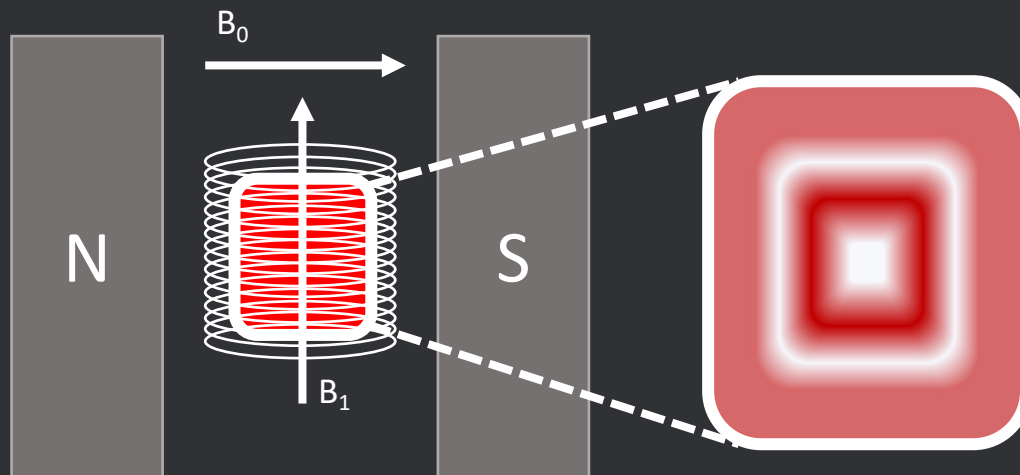
# Low-Field NMR Fingerprinting aided by Artificial Intelligence

MRI APPARATUS



$B_0$ - $B_1$  can be considered homogeneous within each voxel

LOW-FIELD NMR APPARATUS



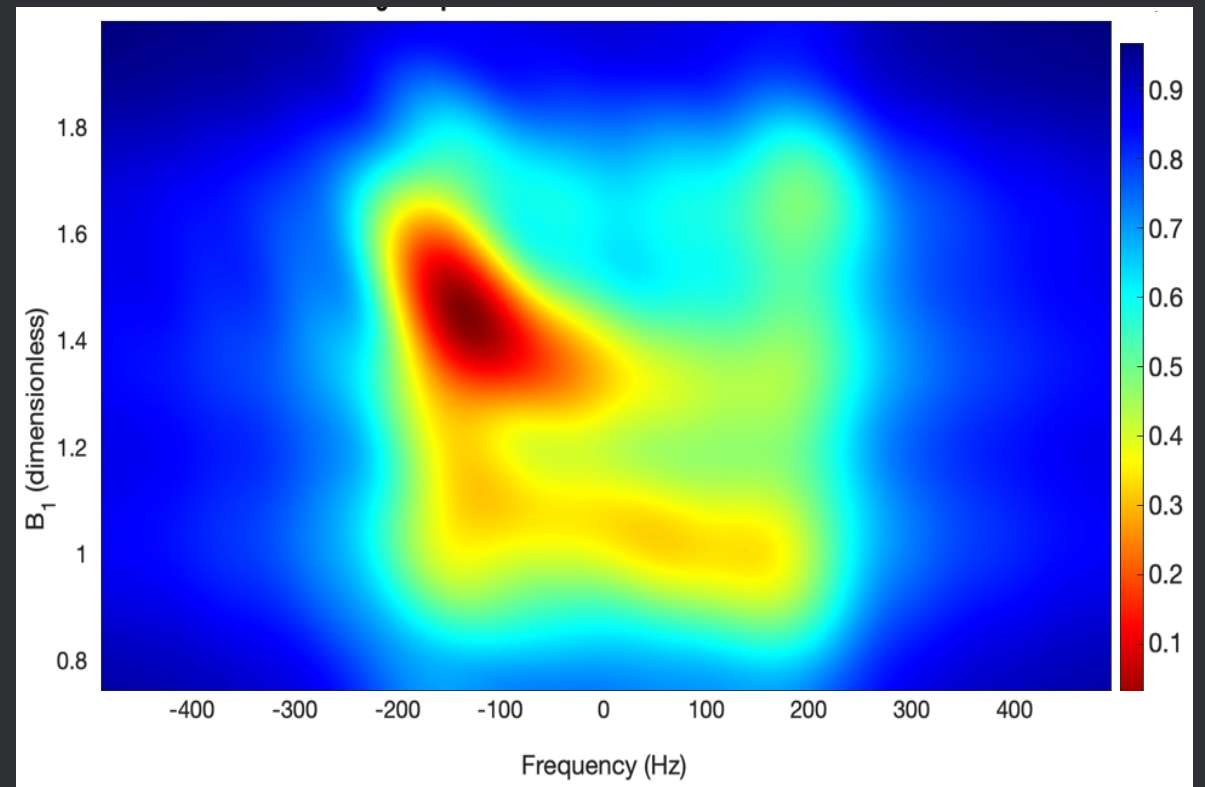
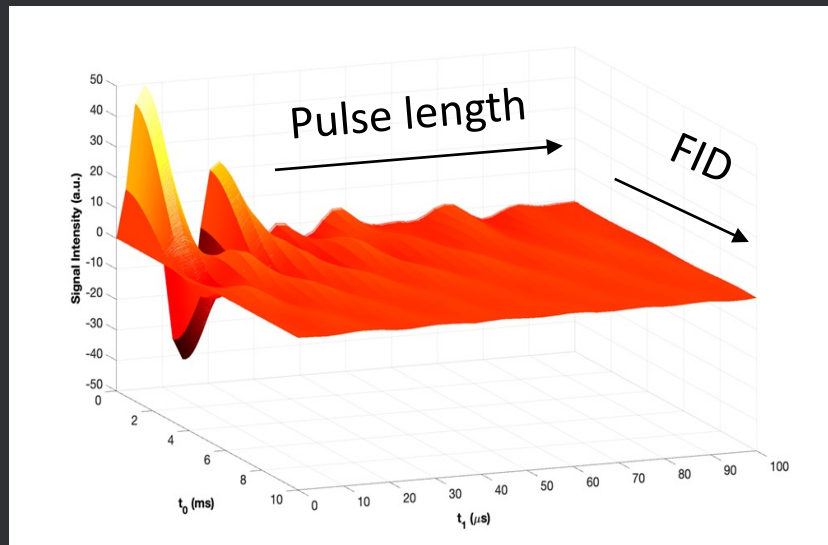
**SPINS DO NOT EXPERIENCE  
HOMOGENEOUS  
 $B_0$  AND  $B_1$**

# Characterization of $B_0$ - $B_1$ correlation function

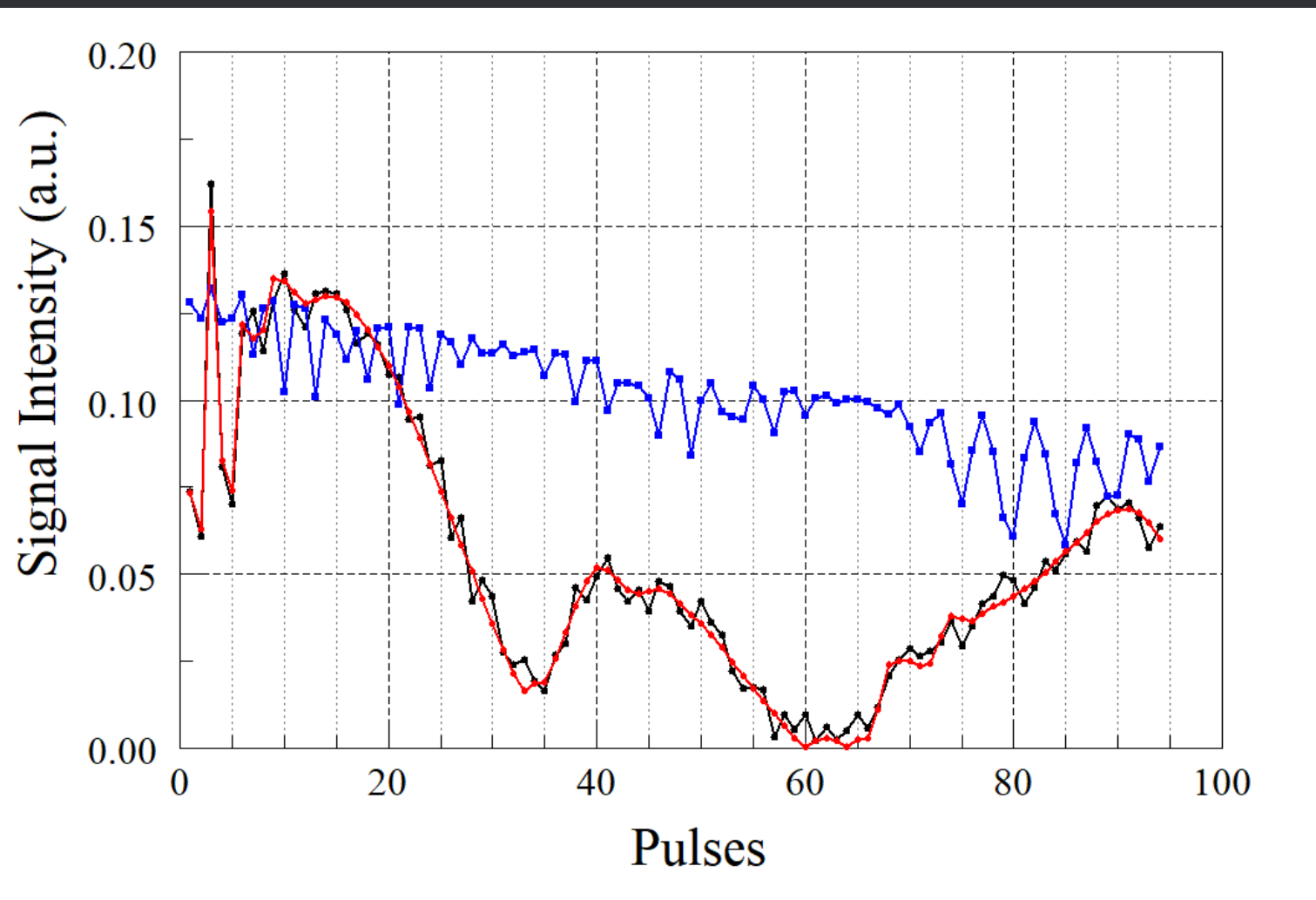
2D FFT

$$S(t_0, t_1) = \iint P(\omega_0, \omega_1) \sin(\omega_1 t_1) e^{(i\Delta\omega_0 t_0)} d\omega_0 d\omega_1$$

$$P(\omega_0, \omega_1)$$



# Low-Field NMR Fingerprinting aided by Artificial Intelligence



**Acquired Signal**

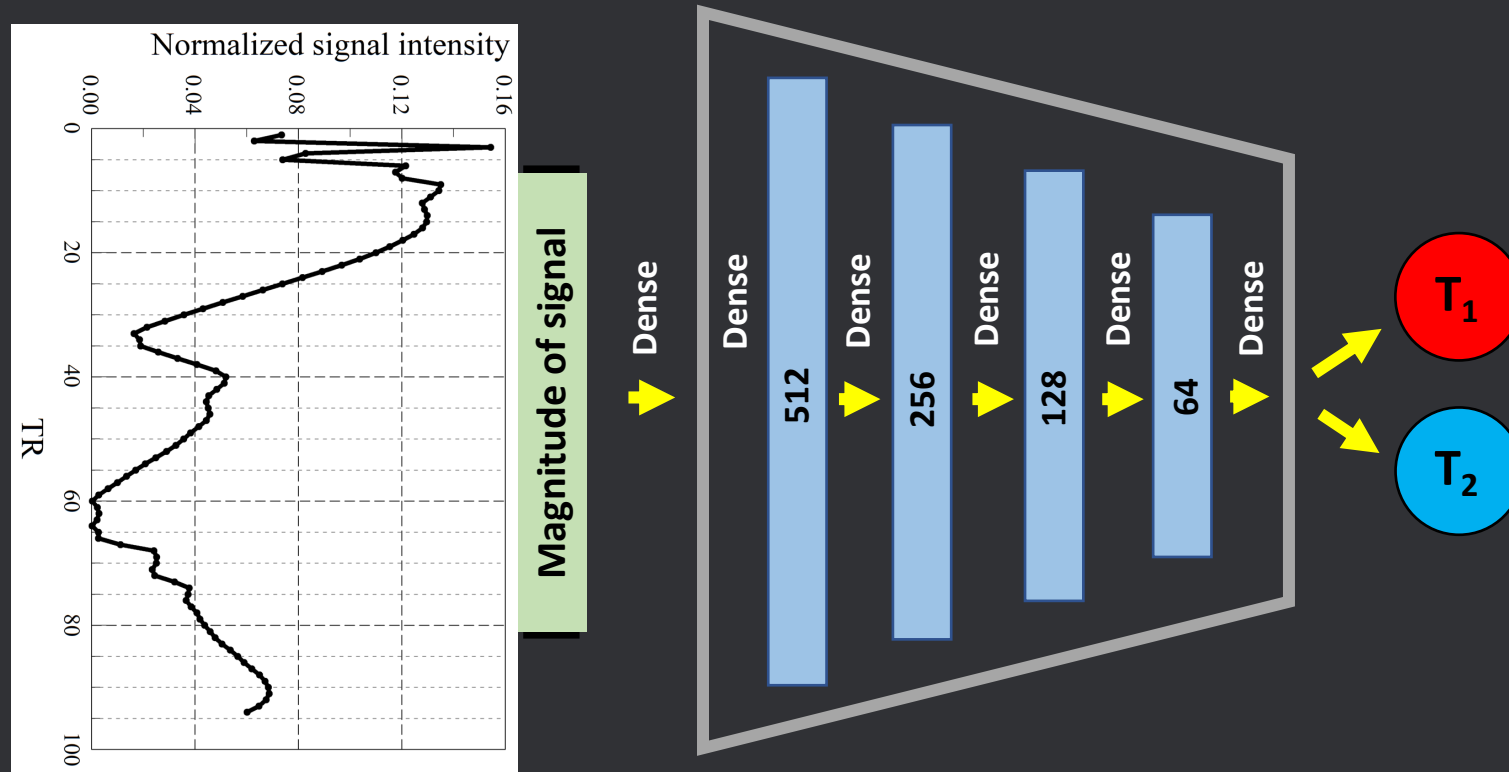
**Simulated Signal  
(using single  $B_0$ - $B_1$ )**

**Simulated Signal  
(using  $B_0$ - $B_1$  distribution)**



# Low-Field NMR Fingerprinting aided by Artificial Intelligence

## Fully Connected Neural Network design



Feed Forward Net - 5 fully connected layers

Rectified Linear Unit (ReLU) as the activation function for the neurons in the first 4 layers

Linear activation function was chosen for the output layer

# Low-Field NMR Fingerprinting aided by Artificial Intelligence

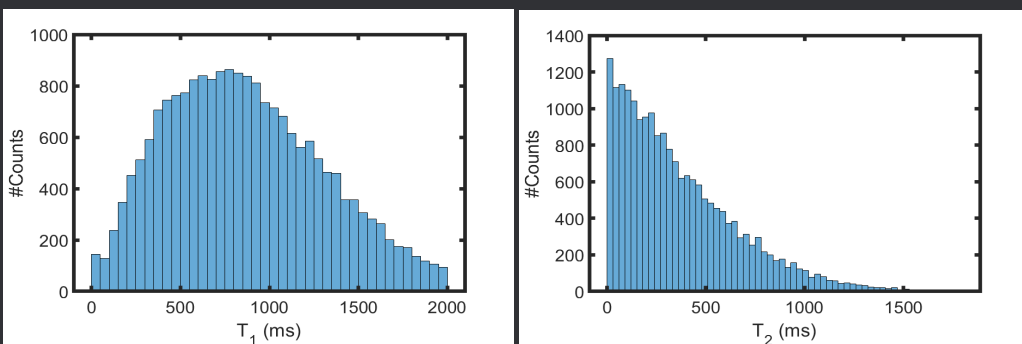
## Training strategy

Training with MARSS synthetic data

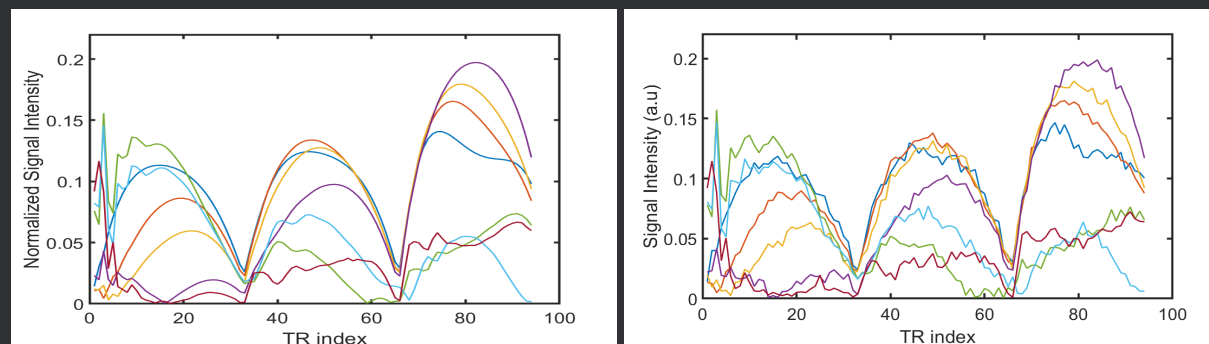
20'000 (T<sub>1</sub>, T<sub>2</sub>) pairs

T<sub>1</sub> (ms)

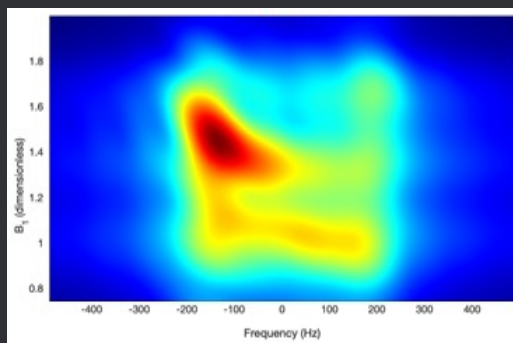
T<sub>2</sub> (ms)



Noise Addition  
(white additive Gaussian)



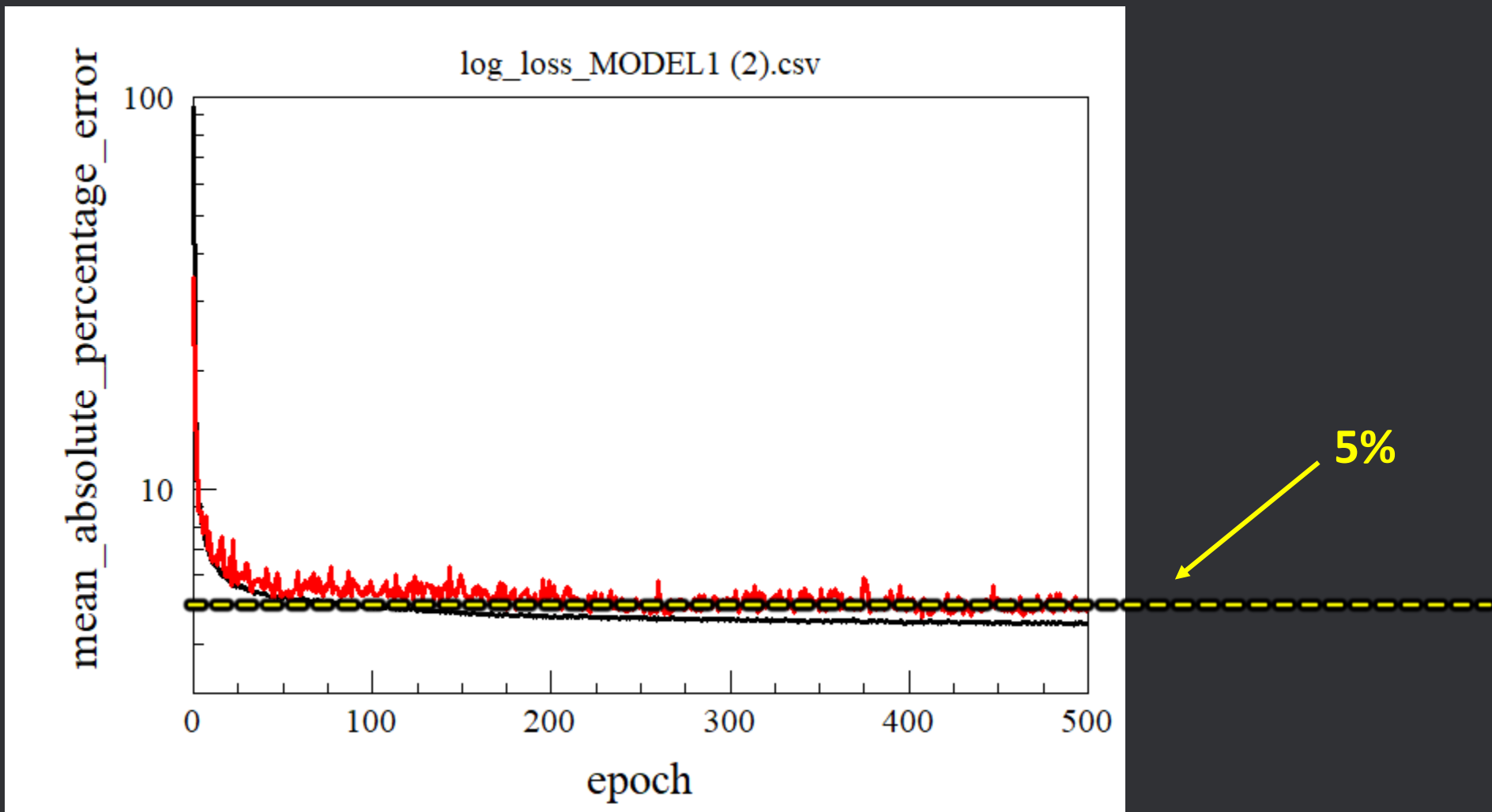
Bo-B<sub>1</sub> Correlation function (84 x 320 MAP)



~3s for 1 simulation (standard PC)  
26880 spin components  
Spin System

~ 2.5 hours for whole dataset generation

training loss / validation loss



# Experimental

H<sub>2</sub>O + CuEDTA

Sample	T1 (ms)	T2 (ms)
CE_1	2.2	1.9
CE_2	12.3	10.4
CE_3	24.1	20.2
CE_4	78.9	66.3
CE_5	301	251
CE_6	729	613
CE_7	1510	1270

Electromagnet JEOL C60 ( $B_0=500$  mT)

Spectrometer KEAll (Magritek, NZ)

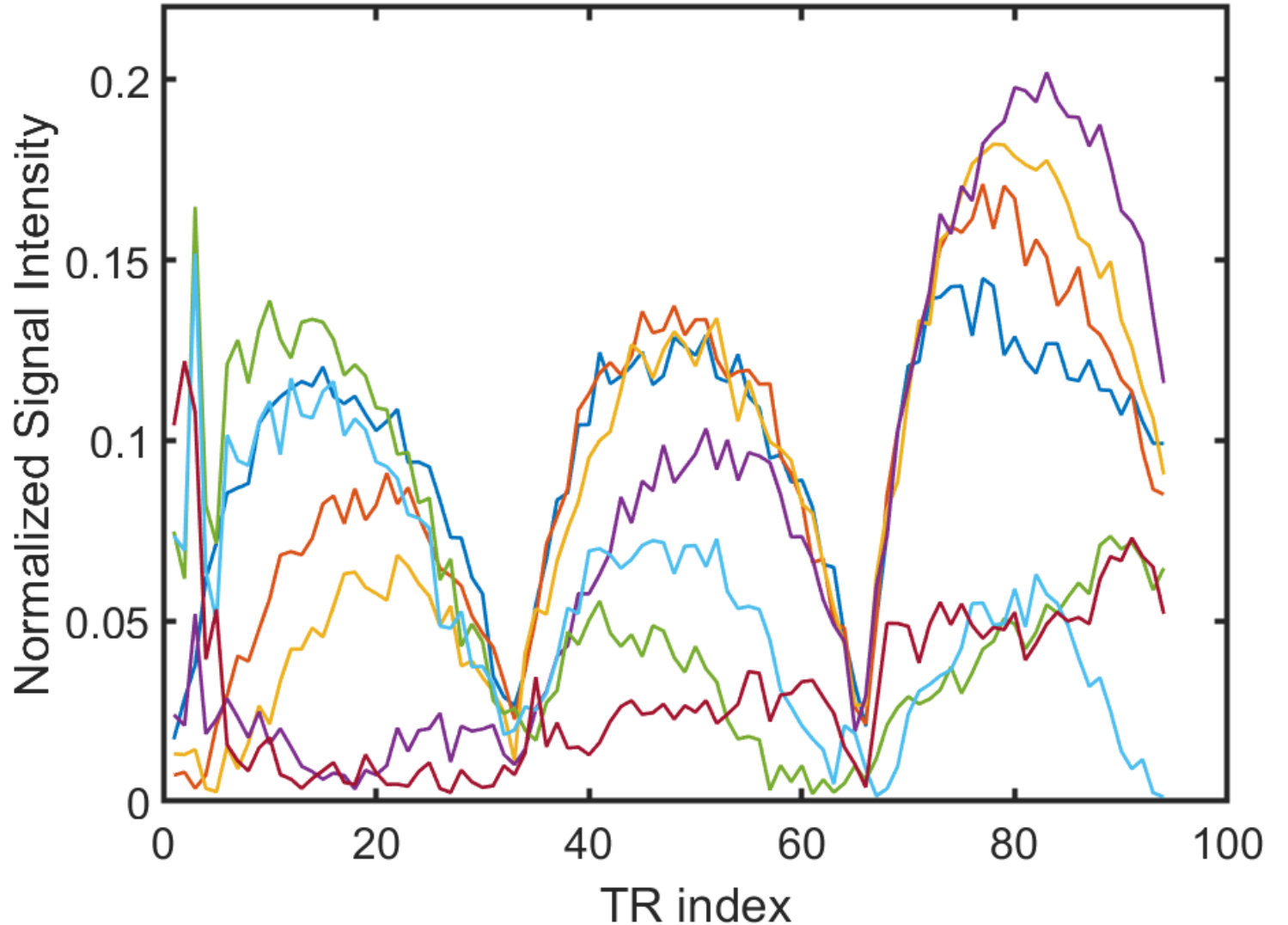
n° of pulses = 95

64 scans

TR fixed at 1 ms

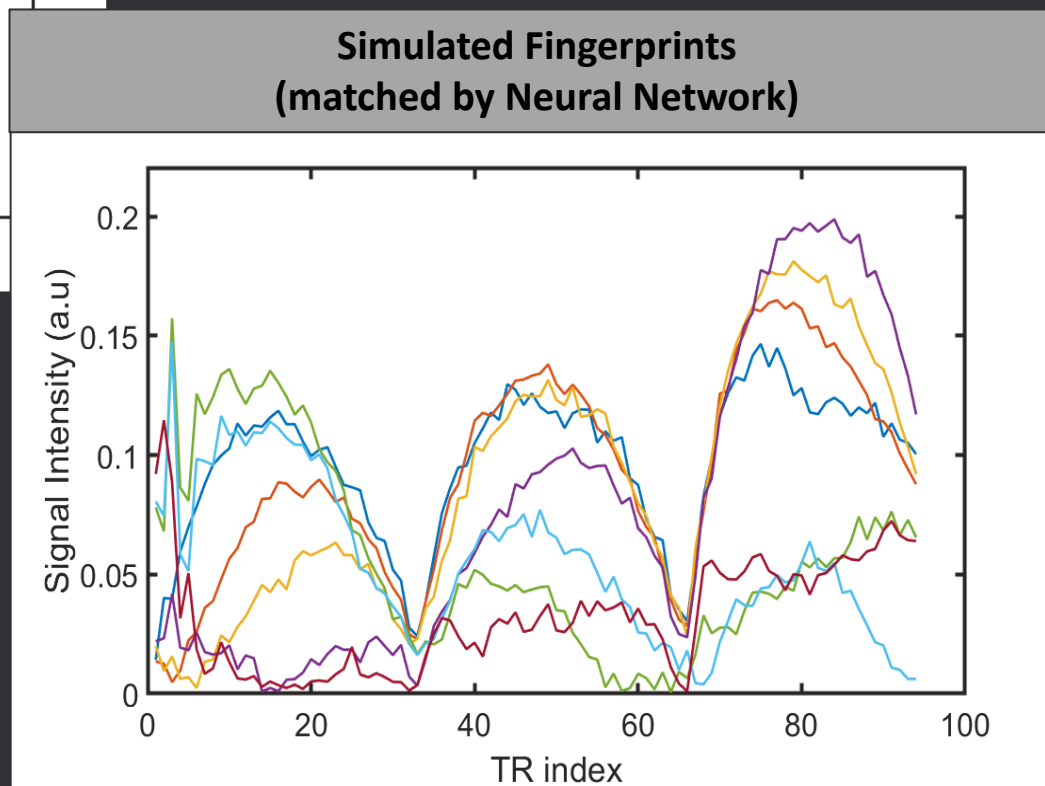
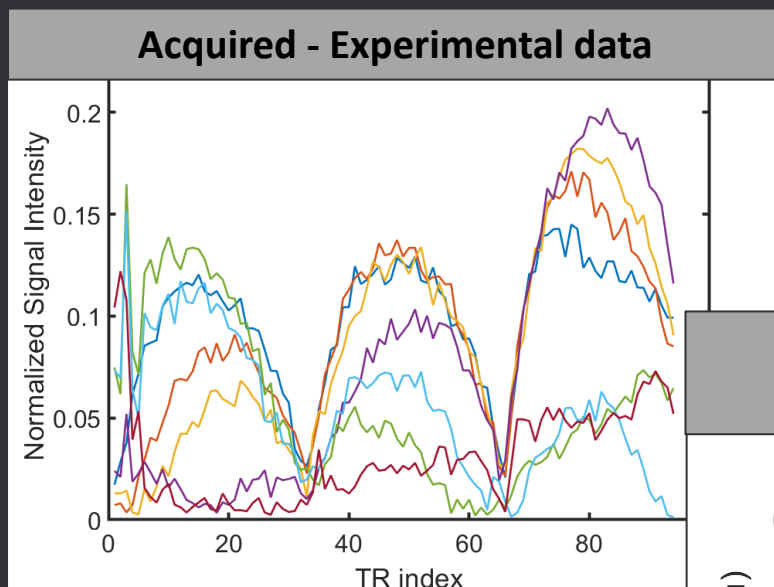
~ 2.5 minutes per fingerprint

## Acquired Data



# Low-Field NMR Fingerprinting aided by Artificial Intelligence

## Data Analysis: Dictionary Matching Vs Neural Network Prediction



T2 Ground	T2 Dict.	T2 NN
1.83	2.00	1.94
10.4	11.0	9.0
20.2	22.0	20.0
66.3	60.0	64.8
251	148	273
613	520	532
1270	1240	1190

T1 Ground	T1 Dict.	T1 NN
2.15	2.00	2.22
12.3	12.0	12.1
24.1	22.0	21.4
78.9	81.0	79.6
301	300	306
730	720	713
1510	1460	1476

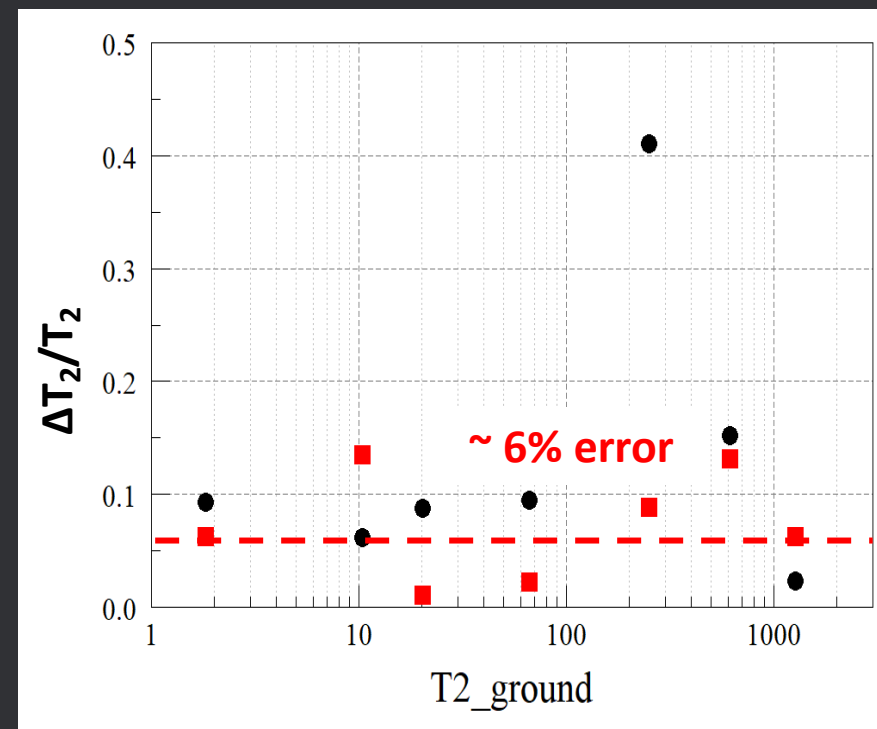
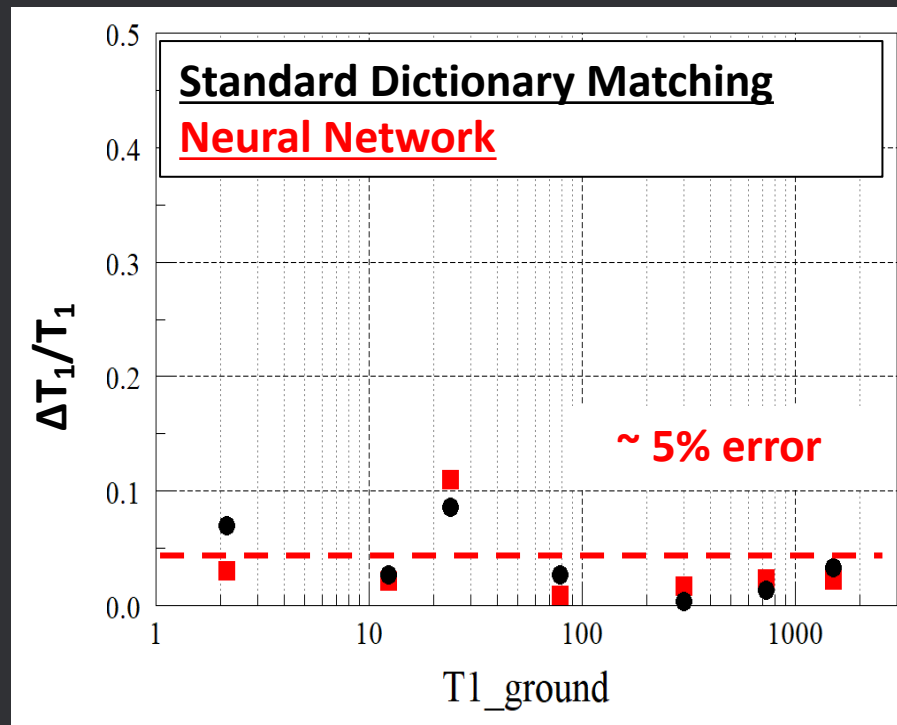
Data values in ms

# Low-Field NMR Fingerprinting aided by Artificial Intelligence

Data Analysis: Dictionary Matching Vs Neural Network Prediction

T1 Ground	T1 Dict.	T1 NN
2.15	2.00	2.22
12.3	12.0	12.1
24.1	22.0	21.4
78.9	81.0	79.6
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1510	1460	1476
T2 Ground	T2 Dict.	T2 NN
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20.2	22.0	20.0
66.3	60.0	64.8
251	148	273
613	520	532
1270	1240	1190

Data values in ms



# CONCLUSIONS

## Low-field Magnetic Resonance Fingerprint

Magnetic Resonance Fingerprinting was demonstrated for low-field Relaxometry devices

Characterization of  $B_0$ - $B_1$  correlation function of the system is requested

A fully connected Neural Network was established to fasten the matching process, achieving the same performance of the standard method

Fast Relaxometry multi-parameter measurements can be performed

# Low-field Magnetic Resonance Fingerprint

Gain Sensitivity to NMR Parameters

Increase the number of encoded Parameters

Extend to multi-components

Self characterization of the hardware ( $B_0 - B_1$ )

Single-sided NMR (Compact and Portable devices)

Translation to

Fast Field Cycling (FFC)

# Further Development

Sequence Design and Optimization

Faster and more Accurate simulation

Neural Network

About dairy products / companies

Portable, low-cost and low-maintenance devices (Low-field)

Fasten the acquisition  
*(real-time in the production line?)*

Automatize for specific applications  
*(not user dependent)*



# Authors have collaborated to presented studies about NMR Fingerprinting



Claudia Testa

Marco Barbieri

Paola Fantazzini

Giovanni Spinelli

Villiam Bortolotti

Anastasiia Nagmutinova

Daniel Remondini



Marco Barbieri

Brian A. Hargreaves

Philip K. Lee

# Thanks for your attention

## Contacts and useful links

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<https://www.unibo.it/sitoweb/leonardo.brizi2/en>

[https://www.researchgate.net/profile/Leonardo\\_Brizi](https://www.researchgate.net/profile/Leonardo_Brizi)



# DICTIONARY

GRID sampling

	T1 (ms)	T2 (ms)	
<b>DICTIONARY</b>	$[2 \div 200]^*$	$[2 \div 200]^*$	<b>20000</b>
	$[201 \div 2000]**$	$[201 \div 2000]**$	<b>entries</b>

\*)  $T_1$  and  $T_2$  were incremented with steps of 1 ms;

\*\*)  $T_1$  and  $T_2$  were incremented with steps of 20 ms.

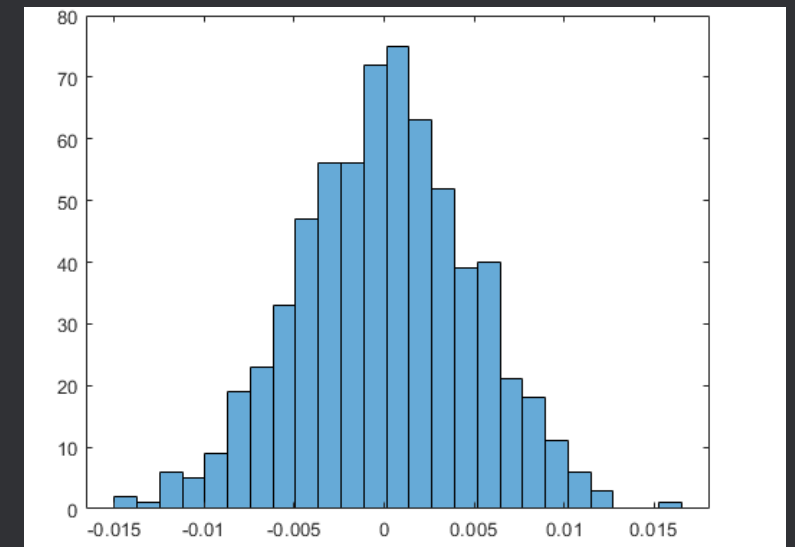
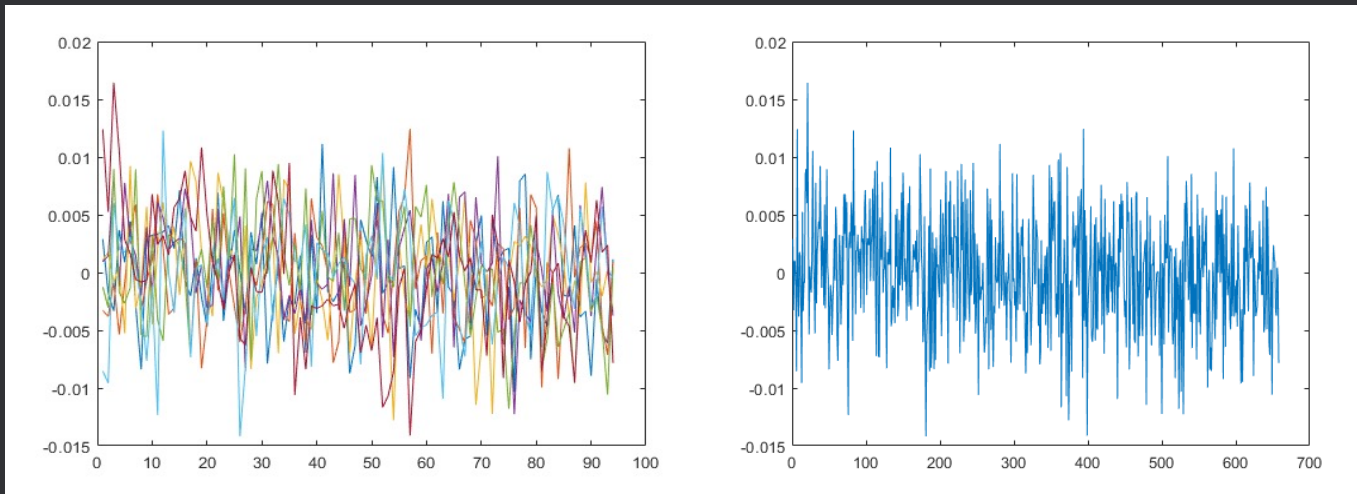
Residuals ~ Noise



Single noise sequence



Noise ~ Gaussian  
 $\mu = 0, \sigma = 0.005$





ELSEVIER

Physica Medica

journal homepage: [www.elsevier.com/locate/efmp](http://www.elsevier.com/locate/efmp)

Original paper

A deep learning approach for magnetic resonance fingerprinting: Scaling capabilities and good training practices investigated by simulations.



Marco Barbieri<sup>a,b</sup>, Leonardo Brizi<sup>a,c</sup>, Enrico Giampieri<sup>d</sup>, Francesco Solera<sup>e</sup>, David Neil Manners<sup>f</sup>, Gastone Castellani<sup>d</sup>, Claudia Testa<sup>a,c,i,j</sup>, Daniel Remondini<sup>a,c</sup>

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<sup>b</sup> Department of Radiology, Stanford University, CA, USA

<sup>c</sup> INFN, Sezione di Bologna, Bologna, Italy

<sup>d</sup> Department of Experimental, Diagnostic and Specialty Medicine, University of Bologna, Bologna, Italy

<sup>e</sup> Deep Vision consulting, Modena, Italy

<sup>f</sup> IRCCS Istituto delle Scienze Neurologiche Bologna, Functional and Molecular Neuroimaging Unit, Bologna, Italy

December 2021

NMR  
IN BIOMEDICINE WILEY

## Circumventing the curse of dimensionality in magnetic resonance fingerprinting through a deep learning approach

Marco Barbieri<sup>1,2</sup> | Philip K. Lee<sup>3</sup> | Leonardo Brizi<sup>1,4</sup> | Enrico Giampieri<sup>5</sup> |  
Francesco Solera<sup>6</sup> | Gastone Castellani<sup>5</sup> | Brian A. Hargreaves<sup>2,3,7</sup> |  
Claudia Testa<sup>1,8</sup> | Raffaele Lodi<sup>8,9</sup> | Daniel Remondini<sup>1,4</sup>

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DOI: 10.1002/mrm.28648

FULL PAPER

Magnetic Resonance in Medicine

## Single-sided NMR to estimate morphological parameters of the trabecular bone structure

Marco Barbieri<sup>1,2</sup> | Paola Fantazzini<sup>1</sup> | Villiam Bortolotti<sup>3</sup> | Fabio Baruffaldi<sup>4</sup> |  
Anna Festa<sup>4</sup> | David N. Manners<sup>5</sup> | Claudia Testa<sup>1,6</sup> | Leonardo Brizi<sup>1,6</sup>

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ELSEVIER

journal homepage: [www.elsevier.com/locate/micromeso](http://www.elsevier.com/locate/micromeso)

FULL PAPER

Magnetic Resonance in Medicine 00:00–00 (2017)

## Bone Volume-to-Total Volume Ratio Measured in Trabecular Bone by Single-Sided NMR Devices

Leonardo Brizi<sup>1,2</sup>, Marco Barbieri<sup>1</sup>, Fabio Baruffaldi<sup>3</sup>, Villiam Bortolotti<sup>4</sup>,  
Chiara Fersini<sup>3</sup>, Huabing Liu<sup>5</sup>, Marcel Nogueira d'Eurydice<sup>5</sup>, Sergei Obruchkov<sup>5</sup>,  
Fangrong Zong<sup>5</sup>, Petrik Galvosas<sup>5</sup>, and Paola Fantazzini<sup>1,2,\*</sup>

**Purpose:** Reduced bone strength is associated with a loss of bone mass, usually evaluated by dual-energy X-ray absorptiometry, although it is known that the bone microstructure also

an impoverishment in the life of elderly people, but also an increase in the costs of health care. Methods to improve the early detection of these diseases are an

Single-sided NMR for the diagnosis of osteoporosis: Diffusion weighted pulse sequences for the estimation of trabecular bone volume fraction in the presence of muscle tissue



M. Barbieri<sup>a,\*</sup>, L. Brizi<sup>a,b</sup>, V. Bortolotti<sup>c</sup>, P. Fantazzini<sup>a,b</sup>, M. Nogueira d'Eurydice<sup>d</sup>, S. Obruchkov<sup>d</sup>, H. Liu<sup>d</sup>, P. Galvosas<sup>d</sup>

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<sup>b</sup> Centro Fermi-Museo Storico della Fisica e Centro Studi e Ricerche "Enrico Fermi", Roma, Italy

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